COMPUTER AIDED DIAGNOSIS OF GLAUCOMA DETECTION USING DIGITAL FUNDUS IMAGE

Ganeshbabu T R,
Department of Electronics and Communication Engineering,
Shri Andal Alagar College of Engineering,
Mamandur, India
ganeshbabutr@gmail.com

Abstract: A robust and cost-effective mass screening may help to detect glaucoma at the earliest which is a major cause of blindness. In this paper, a Computer Aided Diagnosis (CAD) approach for glaucoma detection using retinal fundus images based on clustering techniques is presented. The abnormalities in retinal fundus image are diagnosed using the physiological characteristics of Optic Cup (OC) and Optic Disc (OD). Based on the size of OC and OD, Cup to Disc Ratio (CDR) is computed for the diagnosis. Due to glaucoma, the size of OC increases which increases the CDR as well. In this study, the OD segmentation is achieved by K-Means clustering (KMC) and Hill Climbing Algorithm (HCA) for the selection of K value. Similarly, OC is extracted by exploiting fuzzy C-mean clustering. After segmentation of OC and OD, CDR is computed to diagnose glaucoma. The system is applied to a total of 45 images, and the results indicate the ability of the system for automated mass screening to diagnose glaucoma at the earliest.

Keywords: Glaucoma, Fundus, Optic Cup, Optic Disc, CDR.

I. INTRODUCTION

The major cause of blindness is glaucoma which is a series eye disease in the world. It persists for a long time (chronic disease) and around 90% cases are chronic in nature. As it does not provide any symptoms, it is necessary to check more than two times in a year. The main cause of glaucoma is the pressure inside the eye which is called as intraocular pressure [2]. This pressure damages optic nerve. There are many parameters available to diagnose glaucoma [3]. Chan-Vese model and shape restraint based segmentation of papilla is discussed in [4] using fundus images. The papilla is detected with high accuracy so that the power of discrimination in the extracted shape-based features is very good. Also, it is very robust to noise.

Glaucoma detection based on vessel diameter variation is illustrated in [5]. At first, the registration is done with chamfer matching algorithm, and then differential calculus is employed to detect the vessel centerlines. These profiles are modelled by a Gaussian function to detect vessel diameters.

Morphological based OD localization is discussed in [6] for glaucoma diagnosis. The main circular feature is detected with Hough transform along with gradient image in the horizontal direction. Initially, the brightest areas are isolated by morphological operations.

Level set based CDR computation using fundus images is described in [7]. It uses variational level set and threshold level set for OD and OC segmentation respectively. Finally, the contours are smoothed by elliptical fitting. CDR for glaucoma diagnosis is described in [8] using retinal fundus images based on variational level set and threshold approaches.
In this study, CDR is used for the diagnosis using retinal fundus images. Fundus images show the various characteristics of the retina such as macula, OC and OD. A sample fundus image is shown in Figure 1.

![Fundus Image](image)

**Fig. 1 Fundus Image**

In this study, OD is extracted by KMC with HCA [9], and OC is extracted using FCM [10]. The following section gives the methods used for OD and OC segmentation.

## II. METHODS AND MATERIALS

### A. Image Pre-Processing

In this step, retinal fundus images are preprocessed using anisotropic diffusion [11] filter. The selection of this filter is due to that it does not require the noise pattern, and also it provides contrast. The diffusion equation of this filter is given in Eqn. 1.

\[ I_t = div(c(x,y,t)\nabla I) = c(x,y,t)\nabla I + div c \nabla I \]  

(1)

Where, \( \nabla \) and \( c \) is a gradient and conduction coefficient function respectively. \( div \) and \( t \) denote the divergence operator and iterations respectively. Figure 2 shows the outputs of preprocessing steps.

### B. OD Segmentation

After preprocessing, it is very important to segment OD region at first and then OC segmentation in order to compute the CDR. Before segmentation of OD, the Region Of Interest (ROI) which contains only OD region is cropped.

#### B.1 ROI for OD segmentation

The cropping of ROI region is done automatically based on the intensity of green pixel value in the retinal fundus image. Green pixels provide better contrast than red and blue pixel intensity [12]. The identified maximum intensity points form a cluster of bright region. An ROI of 360x360 pixels is cropped in the original image around the centre of this cluster. Figure 3 shows the retinal fundus image and its ROI.
B.2 Clustering for OD Segmentation

The system uses KMC for OD segmentation. The accuracy of KMC depends on the number of \( k \) seeds. Hence, it is necessary to obtain the value of \( k \). HCA is used for this purpose.

B.2.1 HCA to find number of \( k \) seeds

HCA is applied on the ROI of given fundus image. It is operated on CIE \( l^*a^*b^* \) image [13]. So that the conversion is taken place using RGB to Lab colour conversion in [14]. Based on the 3D colour histogram, the number of \( k \) is identified. Figure 4 shows the colour histogram of three channels in the Lab colour space separately.

After identifying the number of peaks, KMC is applied on the ROI region. It clusters the data based on ‘\( k \)’ value. The OD cluster is identified based on the clustered index of a group of centre pixels. Figure 5 shows the OD segmentation by KMC.
Fig. 4 3D Colour Histogram
C. **OC Segmentation**

The extraction of OC is very difficult in comparison with the segmentation of OD region due to the availability of blood vessels (BVs). OC segmentation consists of two steps; removal of BVs and FCM segmentation.

**C.1 Removal of BVs**

Figure 6 shows the steps followed to remove BVs to segment OC efficiently. The input to this step is the segmented OD region. In [16-18], reverse bi-orthogonal wavelet filter is used to remove the BVs. As this wavelet filter response is same as the structure of BVs, this system also uses this filter for the removal of BVs. Thus, the segmented OD region is only decomposed using one-level decomposition. Using only the low-frequency components for reconstruction, BVs are removed due to that the detail of BV information’s available in the high-frequency bands.

**C.2 OC segmentation by FCM**

In this system, FCM is employed for OC segmentation. FCM is a supervised clustering approach mainly used for clustering data. The input to FCM is the reconstructed image by IDWT in which all BVs are removed. More information on FCM can be found in [19]. As there is no BVs, the number of clusters is set to 3 (background, OD and OC regions).
Fig. 6 Steps to remove BVs
C.3 Computation of OC and OD Diameter

As the segmented regions are irregular in shape, the computation of OC and OD diameter is achieved by mathematical morphological operations. Figure 9 shows the OD region fully enclosed by a rectangle using connected component analysis.

Fig. 8 Optic cup Segmentation

Fig. 9 Rectangle encloses the OD region
To obtain the CDR, the area of an ellipse that fits inside the rectangle is computed. The area is computed using Eqn. 8.

\[
\text{Area} = \pi ab
\]  

(8)

where \(a\) and \(b\) are the major axis and minor axis length. The above Eqn. 8 is applied on both OD and OC segmented regions so that CDR is easily computed.

**III. RESULTS AND DISCUSSION**

A total of 45 images (20 normal retinal fundus images and 25 abnormal retinal fundus images) obtained from Arvind Eye Hospital, Pondicherry, India is used to test the system. A sample normal retinal fundus image and a sample abnormal fundus image with segmented OD and OC regions are shown in Figure 10 (a) and (b) respectively.

From the computed area of segmented OC and OD region, CDR is computed for all 45 retinal fundus images and tabulated in Table 1.
TABLE  1 Computed and gold standard CDR for normal and abnormal fundus images

<table>
<thead>
<tr>
<th>Normal Fundus Image</th>
<th>Gold standard CDR</th>
<th>Computed CDR</th>
<th>Abnormal Fundus Image</th>
<th>Gold standard CDR</th>
<th>Computed CDR</th>
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<tr>
<td>1</td>
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<td>0.55</td>
<td>0.4725</td>
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</table>

From Table 1, it is noted that CDR can be effectively used to diagnose glaucoma. A threshold of 0.35 is used for the diagnosis. If the threshold is above 0.35, the fundus image is said to be abnormal and less than 0.35, it is said to in a normal condition.

A. Analysis by Scatter Plot

Figure 11 shows the scatter plot between the computed CDR and gold standard CDR. This plot is drawn using Mintab statistical tool. It produces a Pearson correlation coefficient of 0.917 that shows a high correlation between both CDRs and repeated regression analysis which is less than 0.0001. A linear regression equation is obtained from the plot. It is given in Eqn. 10.

\[
\text{Gold Standard CDR} = -0.0217 + 1.09 \text{Computed CDR} \quad (10)
\]
It is observed from the Figure 11 that there is a small variation in the computed CDR by the system and the ground truth CDR. This is due to the segmentation problem in OC as they are merged with OD sometimes.

**IV. CONCLUSION**

In this paper, CDR is analyzed to indicate the presence of glaucoma using retinal fundus images. KMC and HCA are employed for the segmentation of OD and whereas FCM is used for OC segmentation. The contour of both OD and OC regions are smoothed by the elliptical fitting approach, and then CDR is computed for 45 retinal fundus images. All images are obtained from Arvind Eye Hospital, Pondicherry. It is concluded that if the CDR is greater than 0.35, the given retinal fundus image is diagnosed with glaucoma and it is less than 0.35; it is a normal eye.

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**REFERENCES**


